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*Video is part of ms*

## **Brain metabolic abnormalities during gait with freezing in Parkinson's disease**

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## ABSTRACT

Introduction: Freezing of gait (FoG) is a debilitating gait disorder in Parkinson's disease (PD). In advanced PD patients with FoG, the supraspinal locomotor network may be dysregulated (relative to similar patients without FoG) during gait. Here, we sought to characterize the metabolism of locomotor networks involved in FoG.

Methods: Twenty-two PD patients (11 with off-drug FoG and 11 without) each underwent two [ $^{18}\text{F}$ ]-fluorodeoxyglucose PET brain scans in the off-drug state: one at rest and another during radiotracer uptake while performing a standardized gait trajectory that incorporated the usual triggers for FoG.

Results: For the 11 freezers, FoG was present for 39% ( $\pm 23\%$ ) of the time during the gait trajectory. The FoG-associated abnormalities were characterized by (i) hypometabolism in frontal regions (the associative premotor, temporopolar and orbitofrontal areas, i.e. Brodmann areas 6 and 8), (ii) hypermetabolism in the paracentral lobule (Brodmann area 5), and (iii) deregulation of the basal ganglia output (the globus pallidus and the mesencephalic locomotor region).

Conclusion: FoG during a real gait task was associated with impaired frontoparietal cortical activation, as characterized by abnormally low metabolic activity of the premotor area (involved in the indirect locomotor pathway) and abnormally high metabolic activity of the parietal area (reflecting the harmful effect of external cueing).

**Abbreviations**

[<sup>18</sup>F]-FDG-PET: [<sup>18</sup>F]-fluorodeoxyglucose positron emission tomography

FEF: frontal eye field

FoG: freezing of gait

MLR: mesencephalic locomotor region

SMA: supplementary motor area

PD: Parkinson's disease

ROI: region of interest

ACCEPTED MANUSCRIPT

## 1. INTRODUCTION

Freezing of gait (FoG) is defined as a brief, episodic absence or marked reduction of forward progression of the feet despite the intention to walk (Nutt et al., 2011). This phenomenon affects about three quarters of people with Parkinson's disease (PD) (Macht et al., 2007). Dopaminergic medications do not alleviate FoG in 15% of patients and produce only partial relief in 44% of patients (Perez-Lloret et al., 2014). Even though severe dopaminergic striatal denervation has been described in models of freezing (even in other parkinsonian syndromes than in idiopathic PD (Park et al., 2009)), imaging studies of patients with PD have shown that the mechanism of FoG also involves non-dopaminergic pathways (Bartels et al., 2006). A better understanding of the neural basis of FoG would probably boost the development of effective therapeutic approaches.

The variable, episodic nature of FoG makes it difficult to study this phenomenon in the laboratory (Schaafsma et al., 2003; Snijders et al., 2008). Furthermore, imaging studies of FoG are technically complex because the freezing occurs during gait (i.e. when the person is in the vertical position, rather than in the horizontal position required for concomitant MRI acquisition) (Bartels and Leenders, 2008; Maillet et al., 2012; Herman et al., 2013; Shine et al., 2013d). Recently, researchers have found new ways of studying FoG by using mental imagery of gait (Snijders et al., 2011; Crémers et al., 2012; Maillet et al., 2015; Peterson et al., 2014a, 2014b) and virtual reality tasks (Shine et al., 2013a, 2013b, 2013c; Shine et al., 2011b). Other functional MRI approaches are based on creating the equivalent of FoG for the upper limbs (Vercruysse et al., 2014a) or performing alternating foot movements in the supine position (Shine et al., 2013a, 2013b, 2013c; Shine et al., 2011b) in order to individualize motor blocks that could be time-locked with changes in brain perfusion. These experiments evidenced corticosubcortical decoupling during freezing, with (i)

hypoactivation of the basal ganglia, thalamus and sensorimotor regions and (ii) hyperactivation of the frontoparietal cortical regions (Shine et al., 2013a; Vercruysse et al., 2014a). Namely, the Brodmann area 6 -including SMA (Snijders et al., 2011; Vercruysse et al., 2014a; Maillet et al., 2015), the pre-SMA (Shine et al., 2013b) and the dorsolateral prefrontal cortex (Vercruysse et al., 2014a)-, is of interest because it is known to be directly involved in locomotor networks used to compensate for gait impairment in patients with PD (Snijders et al., 2011; Shine et al., 2013b; Vercruysse et al., 2014b; Peterson et al., 2014b), potentially via the hyper-direct pathway from the pre-SMA to the STN (Shine et al., 2013d). However, mental imagery and virtual reality do not fully reflect “real life” conditions because (i) the patient’s ability to imagine him/herself performing gait may vary (Cohen et al., 2011; van der Meulen et al., 2014) and (ii) the supine position required for MRI is not physiologically normal for gait because it fails to simulate movement of the centre of gravity during movement (Massion, 1992; Karim et al., 2014).

Otherwise, network-based hypotheses have been tested by using (i) diffusion tensor imaging to study anatomic disconnection (and particularly disconnection from the pedunculopontine nucleus) (Schweder et al., 2010; Tessitore et al., 2012b; Fling et al., 2013; Peterson et al., 2015; Youn et al., 2015) and (ii) the blood-oxygen-level-dependent signal to assess functional reorganization of the default mode and locomotor networks (Pappatà et al., 2011; Tessitore et al., 2012b; Fling et al., 2014; for reviews, see Bartels and Leenders, 2008; Maillet et al., 2012; Herman et al., 2013; Vercruysse et al., 2014a). Lastly, brain atrophy has been measured in patients with FoG, with divergent results (Tessitore et al., 2012a; Sunwoo et al., 2013; Rubino et al., 2014); this may be related to the fact that FoG is frequently associated with cognitive impairment (Herman et al., 2014). Furthermore, cognitive dysfunction can modify brain metabolism (Bohnen et al., 2011; Pappatà et al., 2011). Thus, it is important to recruit non-demented, cognitively matched

patients to better understand the pathophysiology of FoG itself and avoid potential confounding aspects as attentional or executive impairment, that are often linked with FoG (Yogev-Seligmann et al., 2008; Vandenbossche et al., 2011).

In the present study, we adopted a strategy based on current hypotheses about FoG (Nutt et al., 2011; Nieuwboer and Giladi, 2013). In fact, FoG appears to be just one of several abnormalities that occur during continuous gait (Hausdorff et al., 2003; Chee et al., 2009; Vercruysse et al., 2012), including start hesitation (Schaafsma et al., 2003), trembling in place (Schaafsma et al., 2003), sequence effects (Chee et al., 2009) and elevated step variability (Hausdorff et al., 2003). Hence, the gait impairments in patients with FoG are probably more complex than the FoG phenomenon itself since they encompass FoG episodes. Some mental imaging protocols have studied gait disorders in general in freezers (Snijders et al., 2011; Crémers et al., 2012; Maillet et al., 2015). In order to dissociate gait abnormalities and FoG phenomenon, restrictive FoG-time-locked imaging studies have also been performed (Shine et al., 2013a, 2013b), but might therefore fail to observe fundamental metabolic impairments in freezers during gait (Nutt et al., 2011; Nieuwboer and Giladi, 2013; Shine et al., 2013d).

We used here a technique based on the measurement of glucose uptake (a proxy marker for brain metabolism) that has already been used to study (i) gait disorders in progressive supranuclear palsy (Zwergal et al., 2013) and (ii) pure akinesia with gait freezing (Park et al., 2009). Positron emission tomography (PET) of [ $^{18}\text{F}$ ]-fluorodeoxyglucose ([ $^{18}\text{F}$ ]-FDG, a glucose analogue that can cross the blood-brain barrier) is known to reflect the brain cells' metabolism over the 20 to 30 minutes following the injection of the radiotracer. The subsequent stabilization of radiotracer levels enables image acquisition after this timepoint. Hence, if the subject performs actual gait in the 30 minutes following injection of [ $^{18}\text{F}$ ]-

FDG, uptake of the radiotracer will reflect the brain's metabolism during this motor activity, making it a real activation imaging (la Fougère et al., 2010). In the present study, we explored the brain's metabolism during gait with FoG by comparing two matched populations of non-demented PD patients presenting (or not) off-drug FoG during a standardized, 30-minute series of FoG-triggering gait trajectories (referred to hereafter as the "FoG trajectories") (Snijders et al., 2008). We then compared brain activation at rest with brain activation immediately after performance of the FoG trajectories (i.e. reflecting metabolism during uptake of the radiotracer).

We hypothesized that compensatory locomotor networks, involving namely the SMA, could be recruited during this high-level gait task in the non-freezers patients, whereas freezers patients could display less activation of this area. Concerning the subcortical structures (basal ganglia and mesencephalic locomotor region -MLR-), we hypothesized that gait with a real load and intensive proprioceptive afferences could modify the data previously determined by fMRI (Dietz et al., 2002). Finally, we expected a potential deregulation of the compensatory networks in freezers patients.

## 2. METHODS

### 2.1. Subjects

We recruited a group of PD patients with FoG in the off-drug condition (Schaafsma et al., 2003) (the FoG group, n=11) and a matched group of PD patients without FoG (the non-FoG group, n=11). The study's objectives and procedures were approved by the local investigational review board. Each participant gave his/her written consent to participation in the study.

Twenty-two outpatients with PD diagnosed according to Gibb's criteria (1988) were enrolled from the active case file of the Movement Disorders Department at Lille



University Hospital (Lille, France). We first screened PD patients with off-drug FoG (Schaafsma et al., 2003; Espay et al., 2012) (forming the FoG group) on the basis of their answer to item 3 of the FoG questionnaire (Giladi et al., 2009). We next checked that potentially eligible patients displayed FoG episodes during specific FoG trajectories (Snijders et al., 2008) in the off-drug state but not in the “supra-on-drug” state (i.e. after an acute intake of at least one and a half times the usual dose of levodopa) (Schaafsma et al., 2003; Espay et al., 2012). We then included non-freezer PD patients matched for age, gender, cognitive efficiency (according to the Mattis Dementia Rating Scale (Schmidt et al., 1994; Green et al., 1995)) and overall motor severity, in order to form the non-FoG group. The exclusion criteria included the inability to walk unaided in the off-drug condition, the use of deep brain stimulation, the presence of neurological disorders other than PD, dementia (as defined by the Movement Disorders Society criteria (Emre et al., 2007) and by a Mattis Dementia Rating Scale score of 130 or less out of 144 recorded in the 6 months preceding the PET acquisition (Schmidt et al., 1994)) and major depression (according to the DSM IV criteria (American Psychiatric Association., 1994)). To ensure that all FoG episodes were dopasensitive, patients not taking dopaminergic medications as part of their usual therapeutic regimen were excluded from the study. Neuropsychological assessments were performed in on-drug state, including Mini Mental State Examination (Folstein et al., 1975), Mattis Dementia Rating Scale (Green et al., 1995), Hamilton Anxiety Scale (Hamilton, 1959), Montgomery and Asberg Depression Rating Scale (Montgomery and Asberg, 1979) and Lille Apathy Rating Scale (Sockeye et al., 2006) (Table 1).

Although clinical evaluations and PET scans were performed under off-drug conditions, the participants had been on their usual, stable medication regimen for at least 3 months prior to inclusion.

## 2.2. Experimental design

Clinical observations and nuclear medicine procedures were all performed under off-drug conditions (i.e. after the withdrawal of dopaminergic therapy for at least 12 hours) (Langston et al., 1992).

We evaluated the brain's metabolism of [ $^{18}\text{F}$ ]-FDG first at rest and then immediately after continuous gait performed during radiotracer uptake. The time interval between these two acquisitions was between one and four weeks. In the resting condition, the participant lay still in the supine position throughout the 30-minute tracer uptake and stabilization period. A 15-minute PET scan was then performed. In the gait condition, the participant performed FoG trajectories (Snijders et al., 2008) for the 30 minutes immediately following the injection of [ $^{18}\text{F}$ ]-FDG (i.e. during radiotracer uptake and stabilization). The subsequent 15-minute emission scan reflected brain metabolism during the FoG trajectories.

Actual gait was performed for 30 minutes before the PET acquisition because this corresponds to the time required for [ $^{18}\text{F}$ ]-FDG uptake and stabilization in the brain (Lucignani et al., 1993; Shimoji et al., 2004). The patient performed the FoG trajectories (Snijders et al., 2008) throughout the radiotracer uptake period, so that environmental triggers elicited as many FoG episodes as possible.

The FoG trajectory was standardized, as previously described by Snijders et al. (2008): all patients initiated gait and sought to pass through a narrow (80-cm-wide) passage a few metres later. This was followed by a full ( $360^\circ$ ) turn to the right, a full turn to the left, a turn and half ( $540^\circ$ ) to the right, a turn and half to the left, a full turn to the right as quickly as possible, a full turn to the left as quickly as possible, a turn and half to the right as quickly as possible, a turn and half to the left as quickly as possible and then a “go” while counting backwards in threes (starting from a number between 100 and 200), (Figure 1 and

the video in the Supplemental data). The trajectories were performed continuously for the 30 minutes between radiotracer injection and PET acquisition.

*Please insert Figure 1 about here*

## **2.3. Data acquisition and analysis**

### **2.3.1. FoG evaluation**

We used a stopwatch to measure the cumulative duration of FoG episodes during the 30-minute FoG trajectories preceding the PET acquisition (Schaafsma et al., 2003). Each observer tagged the onset of a FoG episode by pressing the stopwatch's button and holding it down until the end of the episode. FoG was considered to be (i) paroxysmal, very small shuffling steps with minimal forward movement (contrasting with the patients' previous steps), (ii) leg trembling in the absence of effective forward motion or (iii) complete akinesia (i.e. no observable motion of the legs) (Schaafsma et al., 2003). The end of each episode of FoG was defined as the time when the patient took an effective step with a relatively normal step length and swing phase (Schaafsma et al., 2003). Data on all subtypes of FoG (start hesitation, trembling in place and FoG when turning, when approaching a narrow gap or when preparing to stop) were pooled. Hence, the percent time with FoG was defined as the ratio of the cumulative duration of FoG episodes to the total test duration (30 minutes). We choose to record the percent time with FoG in order to obtain an objective measure of freezing (Shine et al., 2012); this criterion is more reliable and more accurate than the number of FoG episodes or the mean duration of a FoG episode (Morris et al., 2012).

### **2.3.2. PET data**

All participants underwent PET scans at the same centre (the Nuclear Medicine Department at Lille University Hospital, Lille, France). The same acquisition and image reconstruction procedures were used for the resting and gait conditions in all patients.

#### **2.3.2.1. PET data acquisition**

Data were acquired on an Advance SL PET/CT system (GE Medical Systems, General Electric Company, Chalfont St. Giles, UK) with a 5 mm full-width at half-maximum and a 30 cm transaxial field of view. Participants were instructed to fast before the scans, and the patient's blood glucose level was always checked prior to intravenous injection of between 185 and 198 MBq of [ $^{18}\text{F}$ ]-FDG. Thirty minutes later (i.e. during the radiotracer's stability window from 20 minutes to 90 minutes after injection, reflecting the uptake during the first 20 minutes (Sokoloff et al., 1977)), a low-dose CT scan of the brain was acquired for attenuation correction of the PET data. Emission images were subsequently acquired in three-dimensional mode. The images were reconstructed iteratively using an ordered-subset expectation-maximization algorithm (with two iterations and 21 subsets) in a 256x256 matrix.

#### **2.3.2.2. PET data processing**

The reconstructed [ $^{18}\text{F}$ ]-FDG images were first recorded in Digital Imaging and Communications in Medicine format and then transformed into the Neuroimaging Informatics Technology Initiative format for further processing.

Imaging data were processed and statistically analyzed with SPM5 (Wellcome Department of Cognitive Neurology, London, UK) implemented in MATLAB 7 (Mathworks Inc., Sherborn, MA, USA). Reconstructed [ $^{18}\text{F}$ ]-FDG brain PET images were spatially normalized against the Montreal Neurological Institute (MNI) template (McGill University, Montreal, Canada) using an affine transformation (with 12 parameters for rigid transformations) (Friston, 1995). To increase the signal-to-noise ratio, the images were

smoothed by convolution with an isotropic Gaussian kernel (12 mm full-width at half-maximum). An overall normalization was applied by including each subject's mean global activity as a covariate of no interest. Thus, our patient-by-patient analysis focused on individual differences in regional brain activity as a proportion of overall brain activity.

### **2.3.2.3. PET data analysis**

First, the Talairach applet (Lancaster et al., 1997, 2000) (Research Imaging Institute of the University of Texas Health Science Center San Antonio (UTHSCSA)) was used to determine the location of the nearest grey matter for each significant peak (from the whole-brain analysis). Since the applet uses Talairach space, the coordinates were first translated from MNI space with the MNI-Talairach Coordinate Converter ([www.bioimagesuite.org](http://www.bioimagesuite.org)), as presented in Tables. Next, in order to specifically explore areas of the cortex, brainstem and basal ganglia, we defined a number regions of interest (ROIs): the primary motor cortex, dorsal premotor area, dorsolateral prefrontal cortex, medial prefrontal cortex, posterior parietal cortex, subthalamic nucleus, thalamus, putamen, globus pallidus, caudate nucleus, ventral striatum and MLR, as described by Shine et al. (2013a). The coordinates of each ROI were registered on each PET scan (normalized in MNI space).

### **2.4. Statistical analysis**

When considering clinical data, intergroup differences in continuous variables were evaluated with an unpaired Student's *t* test (for variables with a normal distribution according to the Shapiro–Wilk test) or a Wilcoxon test (for non-normal distributions). A chi-squared test was used for categorical variables. The threshold for statistical significance was set to  $p < 0.05$ . All statistical analyses of clinical data were performed with IBM SPSS for Windows software (version 16.0, IBM, Armonk, NY, USA).

For functional imaging data, we first performed voxel-wise whole-brain analyses by using the flexible factorial design in SPM5. Clusters of at least 30 contiguous voxels with a threshold two-tailed  $p$  value  $<0.005$  were considered to be statistically significant. We included each of the following variables in turn: subject, group (FoG vs. non-FoG) and condition (resting vs. gait). We tested for a main effect of condition (resting vs. gait), a main effect of group (FoG vs. non-FoG) and a group  $\times$  condition interaction. Both increases and decreases in glucose metabolism were analyzed. Post-hoc analyses were based on the “compare-populations one scan/subject” routine. For each voxel, a simple, fixed-effect T test was used to compare the two groups or pairs of conditions. For analyses of ROIs, spherical volumes with a 5 mm radius around the peak coordinates of each ROI were defined and a t test was used to compare the two groups ( $p_{\text{voxel uncorrected}} = 0.005$ ). Lastly, we explored correlations between brain metabolism during gait and the percent time with FoG in the FoG group with a simple regression analysis.

### 3. RESULTS

#### 3.1. Characteristics of the study population

The FoG trajectories performed before the “gait” image acquisition were effective in eliciting FoG episodes. All patients in the FoG group presented FoG episodes, and the mean ( $\pm$  SD) total duration of FoG per patient was 12 ( $\pm 7$ ) minutes (i.e. 39% ( $\pm 23\%$ ) of the 30-minute FoG trajectory; range: 13-77%). No FoG episodes were recorded in the non-FoG group. Gait was more impaired in the FoG group, as shown in Table 1. Due to the FoG itself and the gait impairment between FoG episodes, the number of FoG trajectories completed was obviously lower and more variable in the FoG group. The time needed to complete one FoG trajectory was comprised between 2 and 13 min in the FoG group, compared with 1.5 to 1.8 min in the non-FoG group. Even though the FoG trajectory

(which was the same for all patients) comprised several triggers, most of the FoG episodes in the FoG group were triggered by turning.

*Please insert Table 1 about here*

Intergroup comparisons did not reveal any FoG vs. non-FoG differences in demographic and cognitive data in general or the patients' age, gender, Mini Mental State Examination scores and Mattis Dementia Rating Scale score in particular. There was a non-significant trend toward higher off-drug UPDRS III scores ( $p=0.124$ ) and a longer time since disease onset in the FoG group, when compared with the non-FoG group ( $p=0.007$ ). The two groups differed regarding the gait subscore in off drug (UPDRS III) and freezing subscore (UPDRS II). FoG scores were correlated with motor axial symptoms, as has been observed previously (Giladi et al., 2000, 2001) (Table 2). However, FoG scores (concerning off drug FoG) were not correlated with postural stability nor gait item in on drug (UPDRS II), but with gait item in off drug (UPDRS III).

*Please insert Table 2 about here*

### **3.2. Brain metabolism: [ $^{18}\text{F}$ ]-FDG PET at rest and after the FoG trajectory (Table 3)**

*Please insert Table 3 about here*

#### **3.2.1. Brain glucose metabolism at rest in patients in the FoG and non-FoG groups**

At rest, there was no difference in brain glucose metabolism between the FoG and non-FoG groups.

#### **3.2.2. Brain glucose metabolism after gait (vs. rest) in patients (Figure 2)**

##### **3.2.2.1. The non-FoG group**

In a whole-brain analysis, patients in the non-FoG group displayed post-gait hypermetabolism (vs. rest) in the secondary visual cortex (Brodmann area (BA)18), associative visual cortex (BA19)), premotor cortex (BA6), dorsolateral prefrontal cortex (BA9), somatosensory associative cortex (BA7), cerebellum (culmen), temporoparietal junction (including the superior and middle temporal gyri (BA22 and BA21), supramarginal gyrus (BA40), anterior transverse temporal area (BA41)) and posterior cingulate cortex (BA31) ( $p < 0.005$ ). All the clusters withstood correction for the false discovery rate ( $< 0.05$ ) (Table 3).

*Please insert Figure 2 about here*

The results of the ROI analysis are presented in Table 4. In the basal ganglia, activation after gait (compared with rest) was only significant for the right thalamus and the subthalamic nuclei. There were no differences for the putamen or the caudate nucleus.

*Please insert Table 4 about here*

#### **3.2.2.2. The FoG group**

In a whole-brain analysis, the patients in the FoG group showed post-gait hypermetabolism (vs. rest) in the secondary visual cortex (BA18), premotor cortex (BA6), dorsolateral and anterior prefrontal cortices (BA9 and BA10), primary somatosensory cortex (BA3), cerebellum (the culmen, tonsil, and semi-lunar lobule), basal ganglia, temporoparietal junction (BA40, BA41 and the insula (BA13)) and cingulate cortex (BA30) ( $p < 0.005$ ). All the clusters withstood correction for the false discovery rate ( $< 0.005$  for the first eight clusters and  $< 0.05$  for the following clusters) (Table 3).

The results of the ROI analysis are presented in Table 4. There was overall activation after gait (vs. rest) in the basal ganglia (including the thalamus, subthalamic nucleus and putamen). In contrast, the globus pallidus and the MLR displayed significant



hypometabolism after gait. The FoG group did not activate the medial prefrontal region after gait; in fact, there was a non-significant trend towards deactivation.

### **3.2.2.3. Comparison of brain metabolism after gait in FoG and non-FoG patients (Figure 3)**

When comparing the two groups, the non-FoG group showed greater activation of the temporopolar area (BA38), orbitofrontal area (BA11) and associative premotor cortex (BA8) ( $p < 0.005$ ). Conversely, the FoG group showed greater activation around the intraparietal sulcus in the paracentral lobule (BA5) ( $p < 0.005$ ).

In the ROI analysis, the FoG group showed hypermetabolism (relative to the non-FoG group) in the globus pallidus and left posterior parietal cortex and hypometabolism in the left dorsolateral prefrontal cortex.

*Please insert Figure 3 about here*

The results were generally similar when disease duration and gender were added as covariates (Table 5), with greater metabolic activity after gait in the premotor area, frontal eye fields (FEFs) and somatosensory association cortex in the non-FoG group and in the claustrum, cerebellum and primary visual cortex in the FoG group. Lastly, we observed activation of the temporopolar area and pars orbitalis in the FoG group when disease duration and gender were added as covariates. However, none of the clusters withstood correction for the false discovery rate. Only the 875-voxel cluster located in the right supplemental motor area (BA 6, around (37; 1; 57)) tended to withstand correction for the false discovery rate (0.254) and the family wise error (0.121).

*Please insert Table 5 about here*

### 3.3. Clinical and metabolic correlations (Table 6)

In the FoG group, the percent time with FoG was positively correlated with the activity of the cerebellum, paracentral lobule (BA5) and the right FEF (BA8). Conversely, the percent time with FoG was negatively correlated mainly with the activity in the orbitofrontal area, premotor cortex, the left SMA and temporal lobe. For the study population as a whole, we also found a positive correlation between the UPDRS III gait score and the activity of the cerebellum, FEFs (BA8) and basal ganglia after gait. In contrast, it was negatively correlated with the activity mainly in the orbitofrontal area, premotor cortex, SMAs and temporal lobe (Figure 4).

*Please insert Figure 4 and Table 6 about here*

## 4. DISCUSSION

This [ $^{18}\text{F}$ ]-FDG-PET study is the first to evidence abnormal brain metabolic activation after actual gait in PD patients with FoG. The frontal and parietal cortical FDG uptake seen in non-FoG PD patients differed from that seen in patients with FoG; the latter displayed significant deregulation of the premotor area (notably the premotor cortex and SMA, which are involved in both the indirect cortical locomotor pathway (la Fougère et al., 2010) and attentional mechanisms) and the output of the basal ganglia (namely the globus pallidus-MLR complex). We will first discuss the frontoparietal network and its implication concerning locomotor adaptation according to the environment, then implication of other motor networks (basal ganglia and cerebellar loops) and their involvement in this type of gait.

As previously described for human locomotor control (Jahn et al., 2008a; la Fougère et al., 2010), the classical components of the supraspinal locomotor network are indeed present in our PD patients. In fact, the brain areas involved in PD gait can be grouped together, as

follows: (i) the basal ganglia (involved in motor program selection, (Grillner et al., 2008)), (ii) the cerebellum (involved in rhythm generation, (Grillner, 1985)) (iii) the sensory cortices (for external inputs in general, with a key role in proprioception for motor control in PD (Almeida et al., 2005; Jacobs and Horak, 2006; Schrader et al., 2008; Konczak et al., 2009; Tan et al., 2011)), (iv) the temporoparietal junction (for the multimodal sensory integration of external cues and updating of environmental information via a bottom-up mechanism, (Corbetta and Shulman, 2002; Yang and Mayer, 2014)) and (v) the prefrontal cortex (via a top-down mechanism that regulates pertinent sensory inputs and adapts the motor gait program accordingly (Corbetta and Shulman, 2002; Taylor et al., 2007; Cools et al., 2010)).

Our results are generally consistent with published MRI perfusion data, i.e. in freezers patients an (i) hyperactivation within the paracentral lobule and basal ganglia and (ii) cerebellar dysfunction or (iii) corticosubcortical decoupling, (Shine et al., 2013a; Vercruysse et al., 2014b; Maillet et al., 2015). The differences with regard to the literature data are discussed below.

#### **4.1. Balance inside the frontoparietal network after gait**

First, the results of the whole-brain analysis revealed a premotor vs. parietal contrast, with greater premotor activation in the non-FoG PD group and greater parietal activation in the FoG group. The parietal cortex provides the input for the parietal-premotor and frontoparietal networks (Battaglia-Mayer et al., 2003). In fact, the frontoparietal network may be one of the major functional substrates for modulated gait in PD because it is responsible for integrating external and internal modalities and comparing them with the goal (gait, in this case) (Battaglia-Mayer et al., 2003).

##### **4.1.1. Role of attention**

During gait, the motor program is continuously updated by incoming information. The frontotemporal networks ensure that goal-relevant information receives priority; for example, they will reorient attention if a visual trigger requiring adaptation of the motor program occurs. During modulated gait, the patient has to focus attention on obstacles on his/her path (e.g. when turning in a corridor or upon reaching some stairs) and then adapt his/her trajectory and cadence. However, the patient also has to filter out stimuli that are not behaviourally relevant (e.g. markings on the ground such as threshold strips, or unrelated vocal sounds). Lastly, the most important aspect is the assignment of an appropriate, patient-scaled behavioural response to each stimulus (rather than an exaggerated response in a confined space, for example).

The attentional system includes two networks: the dorsal one (including regions of the intraparietal sulcus, superior parietal cortex, FEF, premotor cortex (SMA), dorsolateral prefrontal cortex) tends to be active during focused, goal-directed attention to a particular target (here gait), whereas the ventral one (including the temporoparietal junction, inferior frontal gyrus, lateral and inferior frontal/prefrontal cortex and anterior insula) is associated with redirecting attention toward stimuli that are relevant to the immediate goal (Corbetta et al., 2008; Asplund et al., 2010; Frank and Sabatinelli, 2012), called stimulus-driven attention. The balance between dorsal and ventral subdivisions of the frontoparietal network requires determining the locus of attention, disengaging and reorienting attention as necessary (Corbetta and Shulman, 2002), especially by determining which stimuli are relevant or not according to the task.

Normally, as task difficulty increases, activity suppression in the ventral network correlates positively with task performance, an effect thought to reflect the gating of irrelevant cues (Frank and Sabatinelli, 2012). It would be expected that during this high-asking attention task with several FoG trajectories, the stimuli integration level would decrease. Indeed, in

the non-freezers patients, this task majority involves the dorsal network, including activation of the FEF, premotor cortex (SMA) and dorsolateral prefrontal cortex. In contrast, in the FoG group, there was a poor frontal activation in FoG, accordingly with less inhibition or gating from frontal to parietal structures (Konishi et al., 1999; Downar et al., 2000, 2001) and then higher activation of the ventral network. Supporting the hypothesis of the impairment of interaction between dorsal and ventral ways in freezers patients, our study showed that the FoG group had less activation of the dorsal pathway than the non-FoG group after gait, mainly in SMA and FEF (Tables 3-5). Moreover, gait scores were positively correlated with the ventral way's activation (inferior frontal gyrus) (Table 6 and Figure 4).

The cingulate cortex was activated by FoG trajectories in both the FoG and non-FoG groups, whereas the temporopolar and orbitofrontal areas were activated in non-FoG patients (relative to FoG patients). Concerning the ventral frontal cortex (ventromedial -BA 10, 11 and 47- and ventrolateral -BA 44, 45 and 47-), its activation after gait was generally positively correlated with the gait score and negatively with the time of freezing. Considering its role in decision making and in stimulus-outcome associations, it could be involved in facilitating changes of behaviour in case of unexpected outcomes (Murray et al., 2007; O'Doherty, 2007). This reversal action, reflecting flexibility, guides selection of the most advantageous choices considering potential positive and negative consequences. Then the ventral frontal cortex could act to signal the task transition and readjust between the dorsal and ventral attentional networks, to prioritize goal or stimulus according to the situation (Shulman et al., 2002; Corbetta et al., 2008). It also could be involved in the transitions between task boundaries as complex gait should not be considered as a continuous activity but as a series of event with interruptions and terminations requiring updating (Bouret and Sara, 2005; Zacks and Swallow, 2007; Corbetta et al., 2008).

It is also important to note that when disease duration and gender were added as covariates, the hypometabolism of temporopolar area after gait decreased in the FoG group – suggesting that the hypometabolism of this area observed in the FoG group is more related to more advanced disease.

#### **4.1.2. Sensory integration: the parietal pole**

The greater activation of parietal areas in patients with FoG may reflect an increased need to rely on external cues because internal integration is impaired (Hallett, 2008). It may also reflect difficulty in resisting external interference (Naismith et al., 2010; Vandebossche et al., 2011). Increased brain activation in the FoG group appears to reflect increased processing of sensory inputs rather than increase in inputs *per se* (which are identical for the two groups). Indeed, if proprioceptive afferences intensity are similar between groups during the FoG-trajectories, the level of deregulation could be the cortical integration of body weight load (Mensink et al., 2014) or proprioception (Tan et al., 2011). Exaggerated processing of sensory inputs might explain the “transient disruptions of locomotor circuitry leading to a motor block” (Nutt et al., 2011) when the sensory integration overloads the locomotor network. Usually, the sensitivity to sensory changes sensitivity is controlled by the task-relevance with insensitivity to task-irrelevant perceptual salient stimuli (de Fockert et al., 2004; Kincade et al., 2005). In case of automatic gait for example, the vestibular and somatosensory cortex showed deactivation, which thus prevents adverse interactions with the spinal pattern and sensory signals (Jahn et al., 2004). This multisensory inhibition, operating during unhindered locomotion, seems impaired in freezers patients. Freezers could display disorders in the process of categorizing stimuli, according to task-relevance or not, showing poor goal-directed and abnormal stimulus-driven activation. FoG could

then be related to an impairment in discriminating what is task (gait) relevant and consider as relevant all distracters.

#### **4.1.3. Premotor differences between non-FoG and FoG groups after gait.**

In both the whole-brain analysis and the ROI analysis, the premotor cortex and SMA were less activated in the FoG group than in the non-FoG group after gait. This finding is in line with literature reports (Snijders et al., 2011; Herman et al., 2013; Shine et al., 2013a). Differences in this region might be due to several different mechanisms – especially those affecting attentional networks and those involved in externally guided (visually guided) movements (Corbetta and Shulman, 2002). In line with our present observations, preferential use of the premotor area in PD has also been described for alternating finger movements (Samuel et al., 1997) and “paradoxical gait” (Hanakawa et al., 1999a), in which visual stimuli improved the PD patients' gait parameters. The FEF that adjusts the visuospatial exploration during gait (by guiding the eye and head movements) might also have a key role here (Pierrot-Deseilligny et al., 2003; Koyama et al., 2004; Brown et al., 2008), as suggested by the correlation between the percent time with FoG and FEF activation. The SMA is classically considered as comprising an anterior region (the pre-SMA, involved in the early stages of motor processing such as motor selection and preparation) and a posterior region (the SMA proper, involved in later stages such as initiation and execution of the motor program) (Matsuzaka et al., 1992; Passingham, 1997; Lee et al., 1999). The difference between FoG and non-FoG patients highlighted here (Figure 2) mainly concerns the posterior SMA; this may reflect that freezers have greater difficulties in initiation and execution than in motor selection. This is suggested (for example) by endless repetition of the motor program during trembling in place - a phenomenon frequently observed during gait initiation (Jacobs et al., 2009b). However, the

coupling between preparation and execution is also included in pathophysiological hypotheses (Jacobs et al., 2009a; Nutt et al., 2011), making it difficult to distinguish between these two components in an analysis of FoG. Lastly, the respective involvements of the preSMA and/or SMA proper might vary as a function of the subtype of freezing (freezing during initiation vs. freezing when turning, for example). One can hypothesize that (i) the preSMA is more involved in gait initiation failure and (ii) the SMA proper is more involved in freezing during movement execution (which was more frequent here). However, our paradigm was unable to distinguish between the metabolic patterns respectively associated with these two subtypes of FoG - although it was noteworthy that freezing in our FoG group occurred mainly when turning.

#### **4.1.4. Pathophysiological hypotheses**

Deregulation of the frontoparietal network in freezers might explain the dual nature of external cueing in FoG. Under ecological conditions, external cues (such as dual tasks) are often disruptive and trigger FoG - probably by overloading the basal ganglia (according to Shine et al.'s model (2011a)) and making gait less automatic. In contrast, external cues can also improve gait parameters (i.e. by increasing step length and lowering step cadence) (Azulay et al., 2006) and might thus decrease FoG (at least temporarily, until the repeated use of the strategy wears off). Hence, external cues (whether auditory or visual) may also help the patient to overcome FoG episodes, when the cues' function is to normalize gait parameters (Nutt et al., 2011). One can hypothesize that the premotor area's role is particularly enhanced when visuomotor modulation is intense. Indeed, when the cues are similar to the standardized gait program, visuomotor coordination is enough to produce relatively normal gait in the FoG group (due to the maintenance of parietal inputs). In contrast, cues that are unrelated to the internal motor program (i.e. external cues that distract attention from redefined motor patterns) will oblige the premotor area to detect



motor errors (i.e. mismatch between the executed motor program and the environment, in terms of speed or direction) and correct them by adapting the motor program via the modulation of the downstream structures. We suggest that this latter mechanism is inefficient in the FoG group.

Furthermore, it is important to note that the brain regions in which metabolic activity was correlated with FoG were largely those correlated with gait impairments in general (Table 6). More severe impairment was related to greater metabolic activity in the FEFs, cerebellum and basal ganglia activity and lower metabolic activity in the premotor and orbitofrontal areas. This finding suggests that there is a continuum between gait disorders and freezing, which might be related to an imbalance between compensatory frontal mechanisms and more basic locomotor networks.

Correlations for time spent with FoG were less unicast (with a positive correlation with FEF and a negative correlation with inferior frontal gyrus, Table 6). Maybe this difference could be explained by the smaller effective (only FoG patients were included here) or could reflect different mechanisms, both impairment and compensation attempt when gait without FoG restart (restart of the dorsal way).

#### **4.2. The ROI analysis: FoG vs. non-FoG differences in activation of the basal ganglia activation.**

In our study, the basal ganglia (namely the putamen) were activated after gait (compared with rest) in the FoG group but not in the non-FoG group. The FoG group showed greater activation of the globus pallidus and thalamus, which may lead to deregulation of the MLR (Lewis and Barker, 2009; Shine et al., 2011a).

Use of the basal ganglia's thalamocortical circuits may manifest itself via "jamming motor execution" in FoG (as seen for trembling in place (Schaafsma et al., 2003)) or by a total arrest in motor execution (as in start hesitation) (Schaafsma et al., 2003).

After gait with FoG, our results evidenced (i) greater activation of the putamen and thalamus (ii) and significant deactivation of the basal ganglia's outputs (the globus pallidus and MLR). The MLR is functionally and anatomically impaired in PD, and the impairment increases with disease progression (Karachi et al., 2010). Functional imaging studies with various paradigms have shown that the MLR is involved in FoG (Snijders et al., 2011; Shine et al., 2013a; Maillet et al., 2015). Although we did not observe intergroup differences in MLR activation in the whole-brain analysis, the ROI analysis showed that this area was significantly deactivated after complex gait in the FoG group. The lack of a significant difference in the present study and the trend to deactivation (in contrast to the study by Snijders et al. (2011) and Maillet et al. (2015)) may be due to methodological differences. Activation of the MLR may be more related to mental imagery of gait initiation, which requires inhibition of the engaged motor program (Jahn et al., 2008b) because motor execution was imagined rather than performed. Furthermore, our study focused on the underlying locomotor pattern associated with FoG and not solely on the narrow time window within which FoG occurs (Shine et al., 2013a). Indeed, gait initiation episodes are much less frequent during actual gait trajectories than during mental imagery paradigms (every 4 to 12 seconds for 25 minutes, for example, in the study by Snijders et al., 2011). It is noteworthy that prefrontal cortex hypoactivation and the absence of MLR hyperactivation were recently described in patients with progressive supranuclear palsy (of which FoG is a cardinal feature) during a modulated gait paradigm (as used in the present study) (Zwergal et al., 2013).

As also reported by Shine et al. (2013a), we observed greater cortical activation in patients with FoG after gait (relative to rest, Table 4). This activation involved not only the primary motor cortex (as in non-FoG patients) but also the premotor area and the posterior parietal cortex. These observations are also suggestive of cortico-subcortical decoupling. When comparing gait with rest within each group, cortical activation was more widespread (i.e. spatially extended) in patients with FoG (although no intergroup differences were noted for the resting condition). This probably corresponds to an attempt by patients with FoG to (i) compensate for impairment of the basal ganglia and (ii) use the external environment to adapt the gait parameters. However, when comparing the two groups after activation by real gait trajectories (i.e. the intergroup contrast), overall activation of the premotor area was less intense in patients with FoG than in patients without FoG. Indeed, cortical activation in patients with FoG was greater in the parietal part of the frontoparietal network (which handles sensory inputs). In contrast, the frontal pole (which handles motor outputs) is poorly activated and is unable to directly shunt the basal ganglia. These observations may explain why our metabolic results (with glucose uptake averaged over 30 minutes of gait) highlighted relatively low activation in the premotor area in patients with FoG, whereas studies exploring perfusion during mental imagery of gait (with the equivalent of FoG-like episodes) reported hyperactivation of the premotor area (Maillet et al., 2015). The premotor activation during FoG or FoG-like episodes may also exist in freezers but is less intense than that observed in non-freezers. These results are consistent with a hypothesis in which the external loop has a compensatory role (Hanakawa et al., 1999a, 1999b; la Fougère et al., 2010) but is not sufficiently effective in PD patients with FoG. Our present results highlighted (i) the low overall activation of the premotor area after gait in PD patients with FoG but (ii) a positive correlation between the percent time with FoG and the metabolism of the FEFs (as similarly shown during upper limb motor blocks by

Vercruysse et al. (2014a)). These observations suggest that PD patients with FoG attempt to use this parietofrontal network but that the latter does not effectively adapt the motor program.

#### **4.3. Is the cerebellar network also involved in gait with freezing?**

Intergroup differences in the frontal and parietal regions might also reflect the involvement of neocerebellar circuits via frontopontine and parietopontine fibres. Indeed, metabolism in the paracentral lobule, superior frontal gyrus and neocerebellar lobes was correlated with the percent time with FoG during the gait task preceding the PET acquisition. These areas belong to the neocerebellar network, which processes sensory information monitors and optimizes movements by using sensory feedback (Jueptner and Weiller, 1998) (via visuomotor coordination, for instance (van der Hoorn et al., 2014)). Interaction with the basal ganglia's thalamocortical loops is required to coordinate the afferent sensory component (the neocerebellar loop) and the efferent motor component (with selection of appropriate muscles and movements). Future research must determine which motor networks are involved in complex gait and whether (as seems likely) communication between them is impaired in patients with FoG.

Even after gender and disease duration were added as covariates, we again observed hyperactivation of the cerebellum, primary visual cortex and claustrum in freezers after gait (reflecting the preferential use of basic rhythmic loops (Tanné-Gariépy et al., 2002; Smith et al., 2012)).

#### **4.4. Putative brain lateralization in FoG**

Our findings are somewhat limited by the question of laterality: in freezers, left-side premotor hypometabolism was observed when studying the effect of group, whereas right-side premotor hypometabolism was highlighted when studying the effect of gait condition. Bilateral involvement is probable but was not unambiguously demonstrated here - perhaps due to the small sample size. Literature studies of paradoxical gait in PD have shown hyperperfusion of the right premotor cortex (Hanakawa et al., 1999), whereas a mental imagery task revealed hyperperfusion of the left supplementary motor cortex in non-freezers (relative to freezers) (Snijders et al., 2011). The left premotor cortex is sometimes considered to have a preferential role in goal-directed movement (Schluter et al., 1998, 2001; Rushworth et al., 2003), although this may have been due to the preferential use of right-hand motor paradigms. In contrast, Bartels and Leenders (2008) suggested that FoG is caused by neuronal circuitry dysfunctions in the right parietal-lateral premotor area (Crémers et al., 2012; Fling et al., 2013; Maillet et al., 2015; Peterson et al., 2014a). In freezers, hypometabolism has been detected in the left premotor area and in the right parietal cortex (Bartels et al., 2006), showing that the both sides of the cortex are affected (albeit in different areas). In fact, there is no clear evidence of laterality of the premotor cortex in action selection (whether in response to visuospatial signals or not) (Wise et al., 1997). For bilateral movements, action selection is probably underpinned by a bilateral network (Horenstein et al., 2009) within which the left and right premotor cortices interact (O'Shea et al., 2007). The laterality of FoG merits further investigation.

#### **4.5. Study limitations**

The present study had several limitations. Firstly, the sample size was small for such a complex disease phenomenon; the lack of statistical power explains why the effect of

group was not corrected for multiple comparisons. Secondly, and even though the FoG and non-FoG groups did not differ significantly in terms of age and motor scores, the disease duration was longer in the FoG group (as is generally observed in this type of patient (Perez-Lloret et al., 2014)). This disparity might explain in part the regional metabolic differences between the groups.

Thirdly, our study was unable to discriminate between the paroxysmal mechanisms corresponding to the various components associated with FoG (such as gait hypokinesia, sequence effects and sudden motor blocks) and the different subtypes of FoG. The injection of perfusion radiotracers (such as  $^{99m}\text{Tc}$ -bicisate) at the time at which each specific subtype of FoG occurs (e.g. FoG during turns) might enable characterization of the corresponding brain perfusion patterns. Lastly, axial symptoms are generally more frequent in freezers (Giladi et al., 2001) - even though the axial subscore was similar in our FoG and non-FoG groups- and may be related to the same pathophysiological mechanisms as FoG itself (Park et al., 2014; Vervoort et al., 2013). Axial symptoms (such as postural stability) are involved in motor control processes related to balance during locomotion. Indeed, axial symptoms form part of the spectrum of gait disturbances encompassing paroxysmal FoG (Heremans et al., 2013), slow execution speed and low step length. Hence, axial symptoms may also account for intergroup differences in brain metabolism after gait (Karachi et al., 2010). These confounding variables must be systematically monitored in future studies.

In PD patients performing arm movements, high movement velocity was associated with hyperperfusion of the premotor and parietal areas (Turner et al., 2003), whereas low movement velocity was associated with hypoperfusion of the left dorsolateral prefrontal and premotor cortices (Carbon et al., 2007). In patients with progressive supranuclear palsy, post-gait differences in brain metabolism (vs. healthy controls) were still significant

after adjustment for gait velocity (Zwergal et al., 2013). Taken as a whole, these data suggest that the premotor hypometabolism observed in freezers may be partly due to a more general gait impairment (including a lower gait speed outside FoG episodes).

#### **4.6. Conclusion**

The present study is the first to demonstrate a characteristic, FoG-associated cortical pattern of metabolic activation in a paradigm including real gait performed by PD patients. In the FoG group, we notably observed (i) hypoactivation of the frontal premotor cortex, (ii) hyperactivation of the parietal cortices and (iii) deregulation of the basal ganglia output (globus pallidus and MLR). Further multimodal imaging studies may help to elucidate the mechanisms underlying FoG in PD patients and prompt the development of techniques for modulating the affected brain networks (such as the frontoparietal and/or neocerebellar networks) involved in visually guided movements (like complex gait) in PD. In parkinsonian patients, the parieto-premotor network could be considered as a compensatory network, that could be overloaded in freezers in different situations such as when they had to reduce their step length (looking at visual cues consisted in white strips placed on the floor) leading to FoG (Iansek et al., 2006; Chee et al., 2009). This task could be further investigated specifically by brain imaging techniques.

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Figure captions

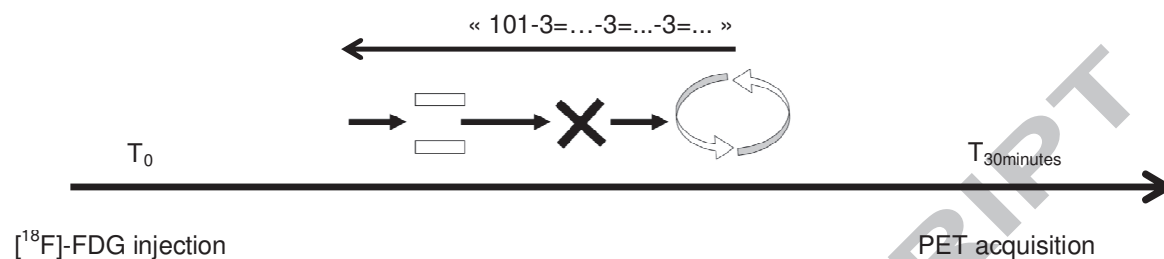
Figure 1: schema of the PET acquisitions

Figure 2: Significant differences ( $p < 0.005$ ) in metabolism when comparing the two experimental conditions (modulated gait vs. resting) in the non-FoG group (left panel) and FoG (right panel) group. Note that both groups of PD patients displayed hypermetabolism in the cerebellum, sensory areas, prefrontal areas, temporoparietal junction and cingulate cortex after performing FoG trajectories. As detailed in Table 4, basal ganglia activation during gait was significant in the FoG group only. The colour scales correspond to the Z-scores.

Figure 3: Significant differences ( $p < 0.005$ ) in metabolism when comparing gait in FoG and non-FoG groups of PD patients. Hypermetabolism was observed in the right rostral SMA, right temporopolar area and right orbitofrontal area in the non-FoG group and in the left intraparietal sulcus and paracentral lobule in the FoG group (from top to bottom). The colour scales correspond to the Z-scores.

Figure 4: Correlations between brain metabolism after the gait session (taking account all the subjects) and gait subscores of Unified Parkinson's Disease Rating Scale part III (off-drug).

**Gait session (see also supplemental video)**

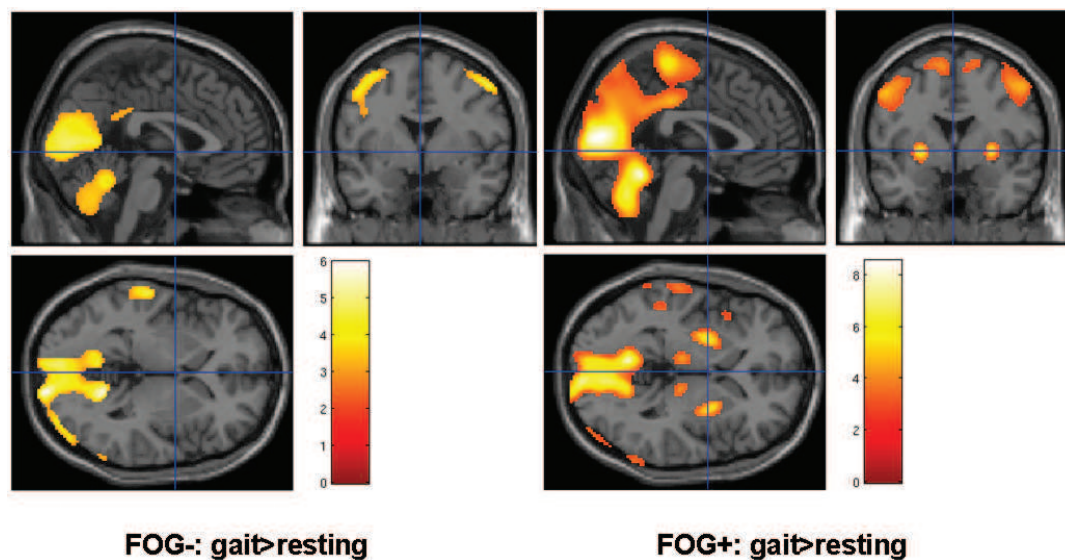


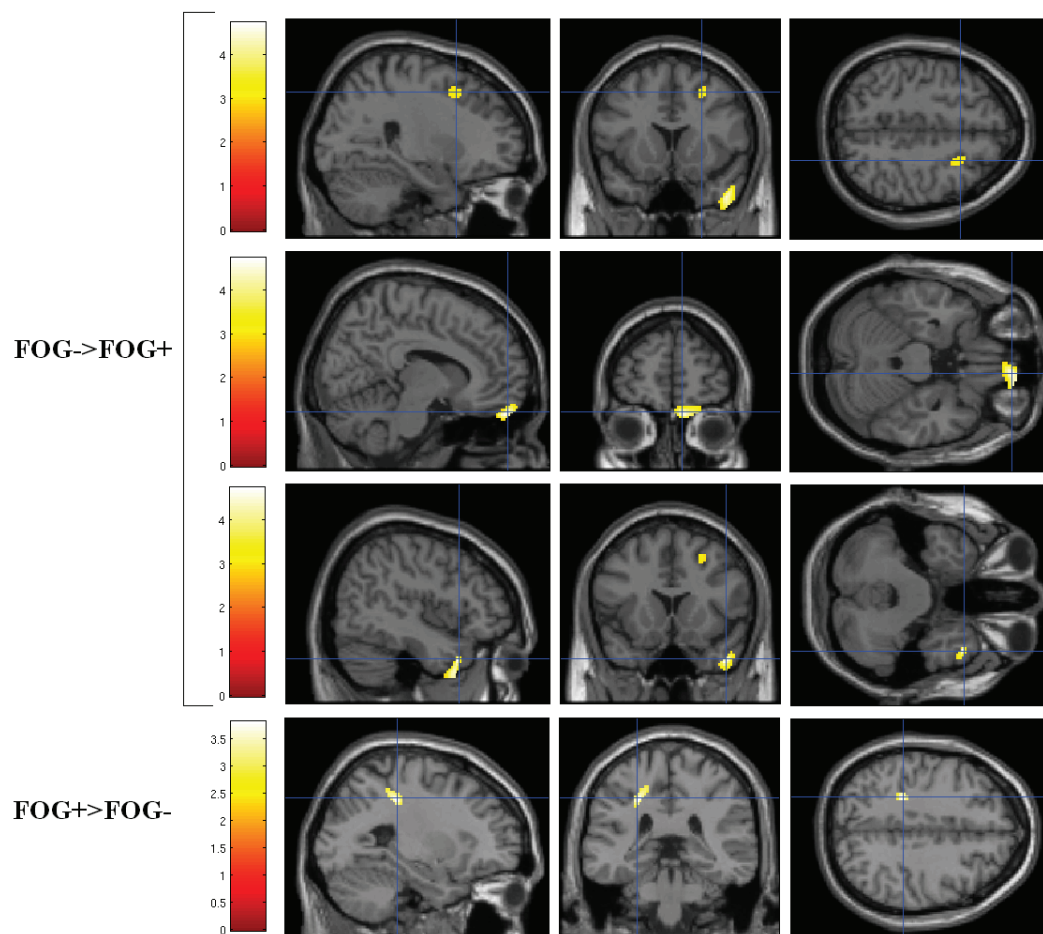
**Rest session**

Comfortably sited  
in a quiet room



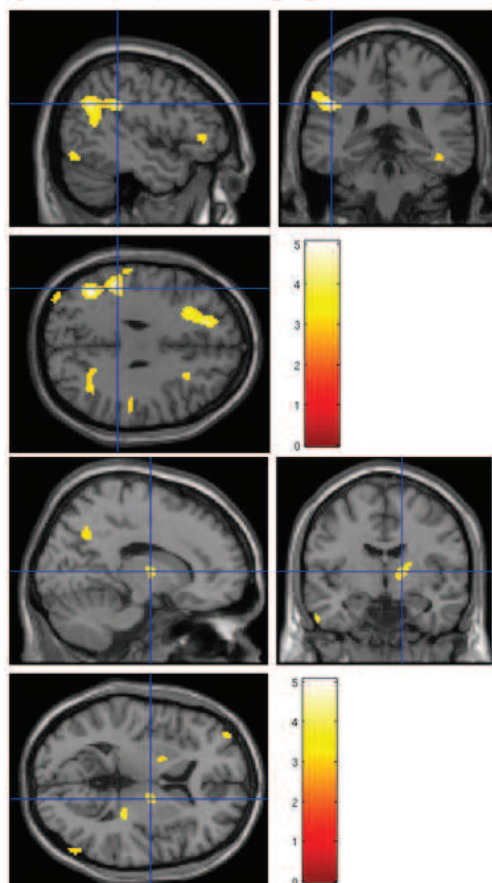
Legend: The double bars indicate the narrow space, the cross indicates a stop (feet together), followed by a further gait initiation (self-initiated), the arrows indicate the series of turns on him/herself (right and left, normal and fast speeds) and finally the return with mental decoupling.





**Correlations with gait subscores (UPDRS 3)**

Positive with mainly the parietal cortex (inferior parietal lobule) and basal ganglia



Negative with mainly the premotor area and the cingulate gyrus

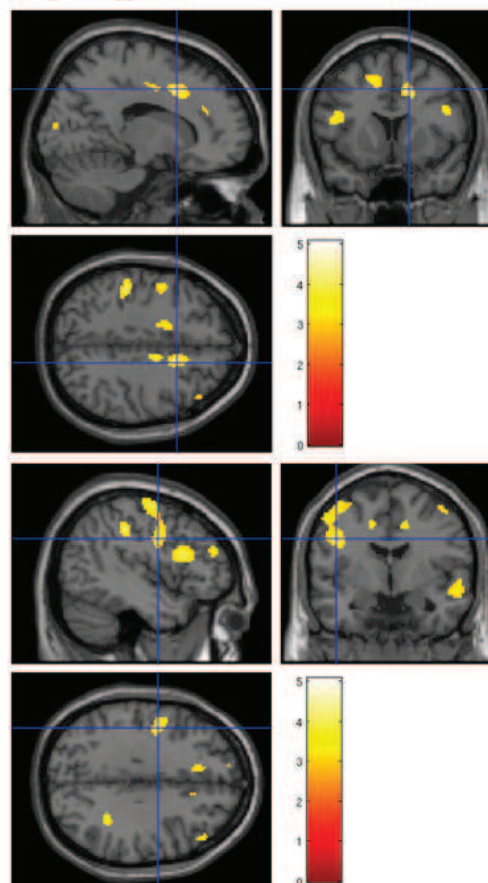


Table 1-A: The demographic, neuropsychological and clinical characteristics of the study subgroups, and statistical comparisons.

N	FoG group 11		non-FoG group 11		p
DEMOGRAPHIC AND DISEASE DATA					
Age (years)	61.36	(4.84)	62.18	(3.37)	0.651
Gender (males/females)	7/4		8/3		0.647
Laterality of predominant motor symptoms (Right/Left)		6/5		4/7	0.669
Mini Mental State Examination score (out of 30)	29.3	(0.9)	29.2	(1.0)	0.702
Mattis Dementia Rating Scale score (out of 144)	137.9	(4.6)	139.3	(3.6)	0.448
➤ Attentional subscore (out of 37)	35.5	(1.5)	35.8	(1.0)	0.637
Hamilton Anxiety Scale score (out of 56)	6.6	(10.0)	2.8	(3.3)	0.308
Montgomery-Asberg Depression Rating Scale (out of 60)	5.5	(5.2)	6.9	(11.6)	0.763
Lille Apathy Rating Scale (out of 36)	-26.4	(5.0)	-24.1	(8.8)	0.554
Unified Parkinson's Disease Rating Scale part III score (off-drug, out of 108)	34.6	(17.3)	25.4	(7.2)	0.124
➤ Gait item (out of 4) -30	2.1	(0.7)	1.1	(0.6)	0.001
➤ Posture item (out of 4) -28	0.8	(1.0)	0.8	(0.6)	0.254
➤ Postural stability (out of 4)-29	0.8	(1.2)	1	(0.9)	0.528
➤ Axial subscore (out of 20)	6.9	(4.0)	3.6	(2.0)	0.720
Unified Parkinson's Disease Rating Scale part II score (on-drug, out of 68)	9.6	(4.0)	8.5	(5.2)	0.392
➤ Gait item (out of 4) -15	1.2	(0.6)	1.1	(0.3)	0.6
➤ Freezing item (out of 4) -14	1.2	(0.6)	0.4	(0.8)	0.001
Time since disease onset (years)	11.0	(2.6)	8.1	(1.9)	0.007
FoG Questionnaire score (out of 24)	12.9	(4.4)	0.2	(0.4)	<0.001
FOG-TRAJECTORIES DATA					
FoG episodes					
Total time with FoG as a proportion of the FoG trajectories	0.39	(0.23)	0	(0.00)	<0.001
Gait parameters between FoG episodes					
Passage through a narrow gap: number of steps for 6 meters	23	(16)	10	(3)	<0.001
Passage through a narrow gap: time for 6 meters (in sec)	13	(14)	8	(2)	<0.001

Dual task with counting: number of steps for 6 meters	62 (37)	10 (3)	<0.001
Dual task with counting: time for 6 meters (in sec)	28 (14)	8 (3)	<0.001

Data are quoted as the mean (standard deviation).

The axial motor subscore was defined as the sum of items 18, 27, 28, 29 and 30 of the Unified Parkinson's Disease Rating Scale part III (speech, rising from a chair, posture, gait and postural stability).

Table 1-B: Antiparkinsonian treatments of the two groups (FoG and non-FoG group). For levodopa equivalent dose daily, the results were presented as mean (standard deviation) and for others treatments, % of patients.

	FoG group	non-FoG group
Levodopa	100%	100%
COMT inhibitors	73%	64%
Dopaminergic agonists	91%	82%
Amantadine	18%	0%
Monoamine oxydase inhibitors	0%	45%
Anticholinergics	0%	9%
Benzodiazepines	27%	9%
Inhibitors of serotonin reuptake	9%	9%
levodopa equivalent dose (mg/day)	1129 (344)	807 (182)

Table 2: correlations between FoG scores and motor scores.

		Percent time with FoG		FoG-Questionnaire	
		Pearson Correlation	Significance	Pearson Correlation	Significance
UPDRS 3 in off drug state	Total motor score	0.506	<b>0.016</b>	0.604	<b>0.003</b>
	Axial subscore	0.564	<b>0.006</b>	0.560	<b>0.007</b>
	Gait	0.754	<b>0.000</b>	0.783	<b>0.000</b>
	Posture	0.445	<b>0.043</b>	0.344	0.127
	Postural stability	0.337	0.135	0.243	0.288
UPDRS 2 in on state	Total daily life score	0.122	0.590	0.229	0.306
	Freezing	0.458	<b>0.032</b>	0.622	<b>0.002</b>
	Gait	0.219	0.340	0.222	0.333
FoG parameters	Percent time with FoG			0.776	<b>0.000</b>
	FoG-Questionnaire	0.776	<b>0.000</b>		
	Item 3 of FoG-Q	0.636	<b>0.001</b>	0.840	<b>0.000</b>

Table 3: Results of an SPM analysis concerning the effect of group and condition and post-hoc analyses.

Cluster	Z-score	pvoxel (unc.)	x	y	z	Functional label	Anatomical label	also known as
<b>EFFECT OF CONDITION: GAIT&gt;RESTING</b>								
72047	6.51	<0.001	4	-52	-18	Cerebellum	Culmen	
			4	-68	-38	Cerebellum	Semi-lunar lobule	
399	4.88	<0.001	-10	-18	4	Thalamus	Mammillary Body	
380	4.73	<0.001	16	-22	6	Thalamus	Ventral Posterior Medial Nucleus	
624	3.94	<0.001	30	0	2	Lentiform Nucleus	Putamen	
126	3.10	0.001	42	24	0	BA47	Inferior Frontal Gyrus	Orbital area
<b>Gait&gt;resting in the non-FoG group</b>								
4495	4.38	<0.001	14	-100	4	BA18	Cuneus	Secondary visual cortex
393	4.12	<0.001	-64	-26	4	BA22	Superior Temporal Gyrus	Primary auditory cortex
70	3.84	<0.001	-24	-88	38	BA19	Cuneus	Associative visual cortex
229	3.79	<0.001	50	-82	8	BA19	Middle Occipital Gyrus	Associative visual cortex
	3.43	<0.001	38	-92	2	BA18	Middle Occipital Gyrus	Secondary visual cortex
109	3.77	<0.001	50	0	54	BA6	Precentral Gyrus	Premotor cortex and Supplementary motor area
280	3.74	<0.001	-40	-4	58	BA6	Precentral Gyrus	Premotor cortex and Supplementary motor area
305	3.60	<0.001	62	-40	24	BA40	Inferior parietal Lobule	
	3.36	<0.001	68	-52	8	BA21	Middle Temporal Gyrus	Middle temporal gyrus
	3.16	<0.001	50	-34	14	BA41	Superior Temporal Gyrus	Auditory primary cortex
123	3.41	<0.001	2	-52	-22	Cerebellum	Culmen	
74	3.28	0.001	8	-44	30	BA31	Cingulate Gyrus	Dorsal posterior cingulate area
	3.11	0.001	12	-56	38	BA7	Precuneus	Somatosensory associative cortex



39	3.16	0.001	-40	6	30	BA9	Inferior Frontal Gyrus	Dorsolateral prefrontal cortex
<b>Gait&gt;resting in the FoG group</b>								
30477	5.55	<0.001	-12	-64	12	BA30	Posterior Cingulate	Agranular retrolimbic area
	5.50	<0.001	4	-52	-18	Cerebellum	Culmen	
	5.49	<0.001	0	-84	12	BA18	Cuneus	Secondary visual cortex
2674	4.66	<0.001	-54	-50	22	BA40	Supramarginal gyrus	
296	4.39	<0.001	-10	-18	6	Thalamus	Medial Dorsal Nucleus	
394	4.38	<0.001	-26	0	0	Lentiform nucleus	Putamen	
316	4.25	<0.001	28	2	0	Lentiform nucleus	Putamen	
179	4.10	<0.001	16	-20	6	Thalamus	Ventral Posterior Medial Nucleus	
1262	3.83	<0.001	52	-2	50	BA6	Precentral Gyrus	Premotor cortex and Supplementary motor area
	3.24	0.001	56	-14	60	BA3	Postcentral Gyrus	Primary somatosensory cortex
	2.86	0.002	48	10	34	BA9	Middle Frontal Gyrus	Dorsolateral prefrontal cortex
417	3.63	<0.001	48	-26	10	BA41	Transverse Temporal Gyrus	Auditory primary cortex
	3.24	0.001	48	-38	18	BA13	Insula	
191	3.40	<0.001	50	-58	-36	Cerebellum	Tonsil	
446	3.30	<0.001	32	44	24	BA10	Middle Frontal Gyrus	Anterior prefrontal cortex
	2.74	0.003	46	32	34	BA9	Middle Frontal Gyrus	Dorsolateral prefrontal cortex
97	2.78	0.003	-34	-82	-40	Cerebellum	Semi-lunar lobule	
<b>EFFECT OF GROUP: non-FoG&gt;FoG</b>								
52	4.03	<0.001	2	-98	28	BA19	Cuneus	Associative visual cortex
77	3.62		-20	0	46	BA6	Middle Frontal Gyrus	Premotor cortex and Supplementary motor area
38	3.19	0.001	54	46	6	BA46	Middle Frontal Gyrus	Dorsolateral prefrontal cortex

82	3.05	0.001	30	-46	42	BA7	Precuneus	Somatosensory associative cortex
38	2.97	0.001	40	-66	20	BA39	Middle Temporal Gyrus	Angular gyrus
<b>EFFECT OF GROUP: FoG&gt;Non-FoG</b>								
118	3.37	<0.001	24	-70	8	BA30	Posterior Cingulate	Agranular retrolimbic area
77	3.11	0.001	-22	-72	8	BA30	Cuneus	Agranular retrolimbic area
73	3.09	0.001	-14	14	-28	BA11	Rectal Gyrus	Orbitofrontal area
60	3.04	0.001	18	18	-28	BA47	Orbital Gyrus	Inferior prefrontal gyrus
57	3.03	0.001	10	-34	30	BA31	Cingulate Gyrus	Dorsal posterior cingulate cortex
30	2.92	0.002	-20	-52	-4	BA19	Parahippocampal Gyrus	
<b>Non-FoG&gt;FoG in the resting condition</b>								
No clusters								
<b>FoG&gt;Non-FoG in the resting condition</b>								
No clusters								
<b>Non-FoG&gt;FoG IN THE GAIT CONDITION</b>								
225	3.86	<0.001	46	16	-36	BA38	Superior Temporal Gyrus	Temporopolar area
232	3.73	<0.001	10	56	-24	BA11	Superior Frontal Gyrus	Orbitofrontal area
77	2.97	0.001	26	14	48	BA8	Middle Frontal Gyrus	Frontal eye fields
<b>FoG&gt;Non-FoG in THE GAIT CONDITION</b>								
125	3.28	0.001	-24	-38	44	BA5	Paracentral Lobule	Somatosensory associative cortex

The “Cluster” column indicates the number of voxels in the significant area. Coordinates (x; y; z) are presented in Talairach space.

Threshold of at least 30 contiguous voxels were applied for clusters, with a two-tailed p value of 0.005. Local maxima more than 8 mm apart were reported only if the corresponding area was different.

First, in greyed out are represented results of gait activation that is hypermetabolic regions during gait by comparing with rest (distinctly between groups, see Figure 1). Secondly are

represented the major results of our study, that is differences between FoG-group and non-FoG group (see Figure 2). Coordinates are given in the Talairach space.

BA: Brodmann area / unc: uncorrected

Table 4: Results of an SPM analysis concerning the ROI.

Group	non-FoG				pvoxel	FoG			pvoxel
					(unc.)				(unc.)
Coordonnates (peak)	x	y	z			x	y	z	
Cortical structures showing activation during gait comparing with rest									
Primary motor cortex	8	-23	64	0.004		2	-26	61	<0.001
	-10	-24	61	0.002		-8	-21	63	<0.001
Dorsal premotor area	14	-9	63	0.029		14	-13	63	<0.001
	-20	-13	64	0.006		-14	-13	63	<0.001
Dorsolateral prefrontal cortex									
	45	29	30	0.006		45	29	30	0.006
	-43	22	29	0.007		-39	21	27	0.001
Medial prefrontal cortex	8	18	33	0.014		No right peak			
	-3	18	33	0.014		No left peak			
Posterior parietal cortex	55	-48	45	0.028		57	-46	46	0.02
	-56	-47	47	0.018		-54	-49	47	0.001
Cortical structures showing deactivation during gait comparing with rest									
Medial prefrontal cortex						No right peak			
						-9	15	28	0.088
Sub-cortical structures showing activation during gait comparing with rest									
Subthalamic nucleus	7	-17	5	0.003		11	-17	5	<0.001
	-7	-17	5	0.005		-9	-17	5	<0.001
Thalamus	7	-15	7	0.003		7	-15	7	0.016

	-7	-15	7	0.008	-7	-15	8	<b>&lt;0.001</b>
Putamen	25	0	5	0.012	27	0	5	<b>&lt;0.001</b>
	-25	0	4	0.033	-25	0	4	<b>&lt;0.001</b>
<b>Sub-cortical structures showing deactivation during gait comparing with rest</b>								
Globus pallidus	12	-4	3	0.024	12	-4	3	<b>0.002</b>
	-12	-2	3	0.025	No left peak			
Caudate nucleus	No right peak				13	14	9	0.082
	No left peak				No left peak			
Ventral striatum	5	9	-4	0.015	5	9	-4	0.022
	-8	3	-2	0.01	No left peak			
MLR	5	-29	-14	0.041	2	-29	-14	0.002
	-1	-29	-14	0.069	-5	-29	-14	<b>&lt;0.001</b>

Coordinates (x; y; z) are presented in Talairach space. Significant p-values are highlighted in bold type.

unc: uncorrected

Table 5: Comparison of brain metabolism in FoG and non-FoG patients after gait by adding covariates (gender and disease duration). Coordinates are given in the Talairach space.

Cluster	Z-score	p (unc.)	x	y	z	Functional label	Anatomical label	also known as
<b>non-FoG&gt;FoG in gait condition with covariates (gender and disease duration)</b>								
510	3.92	<0.001	-36	-58	48	BA7	Superior Parietal Lobule	Somatosensory Association Cortex
100	3.47	<0.001	-42	-34	16	BA41	Superior Temporal Gyrus	
875	3.35	<0.001	37	1	57	BA6	Middle Frontal Gyrus	Premotor cortex and Supplementary motor area
			18	23	46	BA8	Superior Frontal Gyrus	Frontal eye fields
373	3.33	<0.001	29	-67	50	BA7	Superior Parietal Lobule	Somatosensory Association Cortex
			43	-52	46	BA40	Inferior Parietal Lobule	Supramarginal gyrus
83	3.27	<0.001	15	-61	62	BA7	Superior Parietal Lobule	Somatosensory Association Cortex
60	3.11	0.001	13	50	-24	BA11	Superior Frontal Gyrus	Orbitofrontal area
53	3.06	0.001	-34	-91	8	BA19	Middle Occipital Gyrus	Associative visual cortex
67	3.04	0.001	41	1	-40	BA38	Middle Temporal Gyrus	Temporopolar area
			42	7	-31	BA21	Middle Temporal Gyrus	
64	2.91	0.002	-36	-4	56	BA6	Middle Frontal Gyrus	Premotor cortex and Supplementary motor area
40	2.90	0.002	26	42	47	BA8	Superior Frontal Gyrus	Frontal eye fields
85	2.88	0.002	-4	-83	27	BA19	Cuneus	Associative visual cortex
92	2.88	0.002	-18	13	53	BA6	Superior Frontal Gyrus	Premotor cortex and Supplementary motor area
			-15	21	49	BA8	Superior Frontal Gyrus	Frontal eye fields
75	2.87	0.002	8	-83	42	BA19	Precuneus	Associative visual cortex
34	2.84	0.002	-8	31	29	BA32	Cingulate gyrus	Dorsal anterior cingulate cortex
36	2.81	0.003	-50	-64	22	BA39	Middle Temporal Gyrus	Angular gyrus
35	2.69	0.004	-18	-78	25	BA18	Cuneus	Secondary visual cortex
<b>FoG&gt;non-FoG in gait condition with covariates (gender and disease duration)</b>								
294	3.33	<0.001	36	22	-21	BA38	Superior Temporal Gyrus	Temporopolar area
			38	32	-18	BA47	Inferior Frontal Gyrus	Pars orbitalis
44	3.30	<0.001	-23	14	13	Clastrum		
59	3.00	0.001	12	-96	-11	BA17	Lingual Gyrus	Primary visual Cortex
45	2.77	0.003	48	-47	-28	Cerebellum	Anterior Lobe, culmen	

Table 6: Results of an SPM analysis concerning the correlations between metabolic activations and clinical variables (percentage time of FoG and gait items). Coordinates are given in the Talairach space.

Cluster	Z-score	p (unc.)	x	y	z	Functional label	Anatomical label	also known as
<b>POSITIVE CORRELATION with percentage time spent FoG during FoG-trajectory</b>								
74	3.54	<0.001	50	-81	-30	Cerebellum	Posterior Lobe	Tuber
209	3.3	<0.001	2	-30	53	BA5	Paracentral Lobule	Somatosensory Association Cortex
80	3.09	0.001	5	42	47	BA8	Superior Frontal Gyrus	Frontal eye fields
<b>NEGATIVE CORRELATION with percentage time spent FoG during FoG-trajectory</b>								
489	4.54	<0.001	-54	-30	-12	BA20	Inferior Temporal Gyrus	Ventral stream of visual processing
			-59	-9	8	BA22	Superior Temporal Gyrus	Primary auditory cortex
			-53	-12	-7	BA22	Middle Temporal Gyrus	
228	4.41	<0.001	-5	-49	16	BA30	Posterior Cingulate	
164	3.93	<0.001	-24	58	21	BA10	Middle Frontal Gyrus	Anterior prefrontal cortex
84	3.27	0.001	-40	12	17	BA13	Insula	
244	3.18	0.001	-32	-33	55	BA3	Postcentral Gyrus	Primary Somatosensory Cortex
			-44	-29	46	BA40	Postcentral Gyrus	Supramarginal gyrus
			-41	-28	39	BA40	Inferior Parietal Lobule	Supramarginal gyrus
83	3.11	0.001	-18	48	-20	BA11	Superior Frontal Gyrus	Orbitofrontal area
30	3.11	0.001	32	23	-14	BA47	Inferior Frontal Gyrus	Pars orbitalis
							Superior Temporal Gyrus	
140	3.04	0.001	-65	-40	11	BA22	Gyrus	Primary auditory cortex
39	3.01	0.001	-30	-35	-18	BA20	Fusiform Gyrus	Ventral stream of visual processing
125	2.89	0.002	-24	28	-17	BA11	Middle Frontal Gyrus	Orbitofrontal area
			-35	23	-11	BA47	Inferior Frontal Gyrus	Pars orbitalis
								Premotor cortex and Supplementary Motor Area
88	2.85	0.002	-32	-9	49	BA6	Middle Frontal Gyrus	
<b>POSITIVE CORRELATION with gait subscore (UPDRS 3)</b>								
940	3.94	<0.001	-45	-34	29	BA40	Inferior Parietal Lobule	Supramarginal gyrus
			-42	-56	30	BA39	Superior Temporal Gyrus	
103	3.78	<0.001	7	51	43	BA8	Superior Frontal Gyrus	Angular gyrus
			-10	50	37	BA8	Superior Frontal Gyrus	Frontal eye fields
84	3.76	<0.001	-41	-72	-9	BA19	Superior Frontal Gyrus	Frontal eye fields
77	3.62	<0.001	31	63	14	BA10	Fusiform Gyrus	Associative visual cortex
163	3.53	<0.001	-23	-15	36	BA24	Superior Frontal Gyrus	Anterior prefrontal cortex
489	3.51	<0.001	-18	39	26	BA9	Cingulate gyrus	Ventral anterior cingulate cortex
			-27	22	30	BA9	Superior Frontal Gyrus	Dorsolateral prefrontal cortex
266	3.39	<0.001	39	-42	21	BA13	Middle Frontal Gyrus	Dorsolateral prefrontal cortex
			20	-55	34	BA31	Insula	
			36	-54	28	BA39	Precuneus	Somatosensory associative cortex
82	3.39	<0.001	-32	-91	-16	BA18	Superior Temporal Gyrus	Angular gyrus
60	3.31	<0.001	-38	54	9	BA10	Inferior Occipital Gyrus	Secondary visual cortex
354	3.25	0.001	29	-30	9	BA41	Middle Frontal Gyrus	Anterior prefrontal cortex
			41	-31	14	BA41	Insula	
94	3.23	0.001	-6	9	-24	BA11	Superior Temporal Gyrus	Auditory cortex
54	3.13	0.001	-53	-8	-25	BA20	Rectal Gyrus	Orbitofrontal area
204	3.08	0.001	46	26	-6	BA47	Fusiform Gyrus	Ventral stream of visual processing
32	2.98	0.001	-45	33	4	BA45	Inferior Frontal Gyrus	Pars orbitalis
							Inferior Frontal Gyrus	Pars triangularis

79	2.97	0.001	-8	-66	37	BA7	Precuneus	Somatosensory associative cortex
38	2.94	0.001	20	31	37	BA8	Middle Frontal Gyrus	Frontal eye fields
127	2.94	0.002	59	-67	5	BA37	Inferior Temporal Gyrus	Fusiform gyrus
46	2.91	0.002	-40	-84	28	BA19	Superior Occipital Gyrus	Associative visual cortex
40	2.84	0.002	-17	-2	10	Lentiform nucleus		
33	2.81	0.002	-3	-59	2	Cerebellum	Culmen of Vermis	
64	2.81	0.002	63	-26	35	BA2	Postcentral Gyrus	
30	2.81	0.002	-52	-62	0	BA37	Middle Temporal Gyrus	Fusiform gyrus
46	2.76	0.003	-13	-78	-7	BA18	Lingual Gyrus	Secondary visual cortex
<b>NEGATIVE CORRELATION with gait subscore (UPDRS 3)</b>								
310	3.94	<0.001	-37	20	16	BA13	Insula	
351	3.62	<0.001	16	13	39	BA32	Cingulate gyrus	Dorsal anterior cingulate cortex
			12	-4	41	BA24	Cingulate Gyrus	Ventral anterior cingulate cortex
			11	36	19	BA32	Anterior Cingulate Gyrus	Dorsal anterior cingulate cortex
509	3.52	<0.001	-61	-30	16	BA42	Superior Temporal Gyrus	Auditory cortex
145	3.49	<0.001	-43	-28	38	BA40	Inferior Parietal Lobule	Supramarginal gyrus
828	3.49	<0.001	-42	-4	31	BA6	Precentral Gyrus	Premotor cortex and Supplementary motor area
			-51	-6	48	BA4	Precentral Gyrus	
289	3.48	<0.001	44	-25	4	BA22	Superior Temporal Gyrus	Primary auditory cortex
			38	-26	14	BA13	Insula	
299	3.43	<0.001	-13	5	42	BA24	Cingulate gyrus	Ventral anterior cingulate cortex
161	3.32	<0.001	44	16	25	BA46	Middle Frontal Gyrus	Dorsolateral prefrontal cortex
103	3.28	0.001	34	-44	31	BA40	Parietal lobe, Sub-Gyrus	Supramarginal gyrus
110	3.24	0.001	-14	54	24	BA9	Superior Frontal Gyrus	Dorsolateral prefrontal cortex
			-20	57	15	BA10	Superior Frontal Gyrus	Anterior prefrontal cortex
323	3.23	0.001	62	-13	6	BA22	Superior Temporal Gyrus	Primary auditory cortex
			55	-5	13	BA43	Precentral Gyrus	
277	3.19	0.001	-56	-20	-14	BA21	Middle Temporal Gyrus	Middle Temporal Gyrus
			-51	-12	-8	BA22	Superior Temporal Gyrus	Primary auditory cortex
49	3.16	0.001	-43	43	21	BA10	Middle Frontal Gyrus	Anterior prefrontal cortex
120	3.04	0.001	68	-43	16	BA22	Superior Temporal Gyrus	Primary auditory cortex
84	3.02	0.001	-9	28	33	BA9	Medial Frontal Gyrus	Dorsolateral prefrontal cortex
57	2.95	0.002	-32	-20	-20	Hippocampus	Parahippocampal Gyrus	
34	2.92	0.002	33	-65	57	BA7	Superior Parietal Lobule	Somatosensory Association Cortex
51	2.91	0.002	47	35	33	BA9	Middle Frontal Gyrus	Dorsolateral prefrontal cortex
41	2.90	0.002	-52	-35	-11	BA20	Middle Temporal Gyrus	Ventral stream of visual processing
30	2.90	0.002	38	-30	-22	BA36	Limbic lobe	Parahippocampal Gyrus
38	2.84	0.002	20	-85	12	BA18	Middle Occipital Gyrus	Secondary visual cortex
50	2.81	0.002	44	1	54	BA6	Middle Frontal Gyrus	Premotor cortex and Supplementary motor area
49	2.75	0.003	-24	22	-6	BA13	Insula	



- Freezing of gait was related to hypometabolism of premotor area during actual gait
- Freezers presented a hypermetabolism of posterior parietal cortex during gait
- Parietofrontal network was involved in freezing phenomenon
- Basal ganglia overactivation during gait was observed in freezers patients
- The balance between external and internal signals may fail during freezing